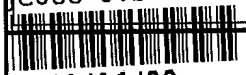


34-27-00

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PATENT APPLICATION TRANSMITTAL LETTER (Small Entity)	Docket No. P1308USA
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 04/26/00

TO THE ASSISTANT COMMISSIONER FOR PATENTS

Transmitted herewith for filing under 35 U.S.C. 111 and 37 C.F.R. 1.53 is the patent application of:

Kuiken

For: **HIGH PROFILE MULTIAXIAL PROSTHETIC FOOT**

JC530 U.S. PTO
 09/558570
 04/26/00

Enclosed are:

- ☒ Certificate of Mailing with Express Mail Mailing Label No. **EJ216456561US**
- ☒ Four sheets of drawings.
- ☐ A certified copy of a _____ application.
- ☒ Declaration ☒ Signed. ☐ Unsigned.
- ☒ Power of Attorney
- ☐ Information Disclosure Statement
- ☐ Preliminary Amendment
- ☒ Non-Profit Verified Statement(s) to Establish Small Entity Status Under 37 C.F.R. 1.9 and 1.27.
- ☒ Other: **Express Mail Certification; Return Postcard**

CLAIMS AS FILED						
For	#Filed	#Allowed	#Extra		Rate	Fee
Total Claims	22	- 20 =	2	x	\$9.00	\$18.00
Indep. Claims	3	- 3 =	0	x	\$39.00	\$0.00
Multiple Dependent Claims (check if applicable) <input type="checkbox"/>						\$0.00
BASIC FEE						\$345.00
TOTAL FILING FEE						\$363.00

- ☒ A check in the amount of **\$363.00** to cover the filing fee is enclosed.
- ☒ The Commissioner is hereby authorized to charge and credit Deposit Account No. **07-0181** as described below. A duplicate copy of this sheet is enclosed.
 - ☐ Charge the amount of _____ as filing fee.
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 - ☒ Charge any additional filing fees required under 37 C.F.R. 1.16 and 1.17.
 - ☐ Charge the issue fee set in 37 C.F.R. 1.18 at the mailing of the Notice of Allowance, pursuant to 37 C.F.R. 1.311(b).

Dated: **April 26, 2000**


 Signature

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**EXPRESS MAILING CERTIFICATE
UNDER 37 C.F.R. § 1.10**

EL216456561US
"Express Mail" Mailing Number

April 26, 2000
Date of Deposit

I hereby certify that a Patent Application Transmittal (Small Entity); a Declaration & Power of Attorney; a check for \$363.00; a Specification (16 pages); Drawings (4 sheets); a Small Entity Statement for Non-Profit Organization; and a return post card are being deposited with the United States Postal Service "Express Mail Post Office to Addressee" service under 37 C.F.R. § 1.10 on the date indicated above, addressed to the Assistant Commissioner for Patents, Box: Patent Application, Washington, D.C. 20231.

Jose L. Fontanez
(Typed or Printed Name of
Person Mailing Application)


(Signature of Person
Mailing Application)

(Docket: P1308USA)

**VERIFIED STATEMENT (DECLARATION) CLAIMING SMALL ENTITY
STATUS (37 CFR 1.9(f) AND 1.27 (d)) - NONPROFIT ORGANIZATION**

Docket No.
P1308USA

Serial No.

Filing Date

Patent No.

Issue Date

Applicant/ **KUIKEN, Todd A.**
Patentee:

Invention: **HIGH PROFILE MULTIAXIAL PROSTHETIC FOOT**

I hereby declare that I am an official empowered to act on behalf of the nonprofit organization identified below:

NAME OF ORGANIZATION: Rehabilitation Institute of Chicago

ADDRESS OF ORGANIZATION: 345 East Superior Street
Chicago, Illinois 60611
TYPE OF NONPROFIT ORGANIZATION:

- ☐ University or other Institute of Higher Education
- ☒ Tax Exempt under Internal Revenue Service Code (26 U.S.C. 501(a) and 501(c)(3))
- ☐ Nonprofit Scientific or Educational under Statute of State of The United States of America
Name of State: _____ Citation of Statute: _____
- ☐ Would Qualify as Tax Exempt under Internal Revenue Service Code (26 U.S.C. 501(a) and 501(c)(3)) if Located in The United States of America
- ☐ Would Qualify as Nonprofit Scientific or Educational under Statute of State of The United States of America if Located in The United States of America
Name of State: _____ Citation of Statute: _____

I hereby declare that the above-identified nonprofit organization qualifies as a nonprofit organization as defined in 37 C.F.R. 1.9(e) for purposes of paying reduced fees to the United States Patent and Trademark Office regarding the invention described in:

- ☒ the specification to be filed herewith.
- ☐ the application identified above.
- ☐ the patent identified above.

I hereby declare that rights under contract or law have been conveyed to and remain with the nonprofit organization with regard to the above identified invention.

If the rights held by the above-identified nonprofit organization are not exclusive, each individual, concern or organization having rights to the invention is listed on the next page and no rights to the invention are held by any person, other than the inventor, who could not qualify as an independent inventor under 37 CFR 1.9(c) or by any concern which would not qualify as a small business concern under 37 CFR 1.9(d) or a nonprofit organization under 37 CFR 1.9(e).

Each person, concern or organization to which I have assigned, granted, conveyed, or licensed or am under an obligation under contract or law to assign, grant, convey, or license any rights in the invention is listed below:

- ☒ no such person, concern or organization exists.
☐ each such person, concern or organization is listed below.

FULL NAME

ADDRESS

☐

Individual

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Small Business Concern

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FULL NAME

ADDRESS

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Individual

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Small Business Concern

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Nonprofit Organization

Separate verified statements are required from each named person, concern or organization having rights to the invention averring to their status as small entities. (37 CFR 1.27)

I acknowledge the duty to file, in this application or patent, notification of any change in status resulting in loss of entitlement to small entity status prior to paying, or at the time of paying, the earliest of the issue fee or any maintenance fee due after the date on which status as a small entity is no longer appropriate. (37 CFR 1.28(b))

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code, and that such willful false statements may jeopardize the validity of the application, any patent issuing thereon, or any patent to which this verified statement is directed.

NAME OF PERSON SIGNING:

Nancy E. Paridy

TITLE IN ORGANIZATION:

General Counsel

ADDRESS OF PERSON SIGNING:

Rehabilitation Institute of Chicago345 East Superior StreetChicago, Illinois 60611

SIGNATURE:

Nancy E. Paridy

DATE:

4/26/00

HIGH PROFILE MULTIAXIAL PROSTHETIC FOOT

Field of the Invention

The present invention relates to a high-profile prosthetic foot that provides up to 180° of medial-lateral rotation with respect to the prosthesis frame and also provides energy storage capabilities. The present invention further relates to a prosthetic ankle joint having an adjustable range of medial-lateral rotation about the prosthesis frame.

Background of the Invention

A prosthetic foot must provide stable support to the user under a variety of conditions. Such conditions include a variable stride and a range of different activities. In particular, a prosthetic foot has long been sought that can provide stable support for a user who is walking on an ever changing terrain, such as that encountered in normal daily activity. To achieve this objective, a prosthetic foot would ideally provide a range of motion in a medial-lateral direction. It is also desirable that the prosthetic foot has energy storage capabilities to provide a more normal gait.

Dynamic response prosthetic feet are preferred for active amputees. The energy storage capabilities of the feet give them a spring-like functionality, which improves the feel and overall function of the prostheses. Two widely used types of prosthetic feet are high profile dynamic feet and low profile multiaxial feet.

High profile dynamic feet consist of a long L-shaped piece of material attached to a base plate. The L-shaped piece of material may be alternatively referred to as a frame. Typically, the frame is elastic and therefore provides some energy storage capability. Generally, the frame is a composite, such as a carbon fiber laminate or a polymeric material. At present, all high profile dynamic feet have a rectangular cross section relative to the frame and therefore movement of the footplate is typically limited. Such high profile dynamic feet have advantages because of their high-energy storage capability. High-energy storage occurs in the frame of the prosthesis. High profile dynamic feet have the longest frame, and thus act as the biggest springs and, accordingly, store the most energy. However, high profile dynamic feet also present some drawbacks. Principally, the high profile dynamic feet have no ankle motion and therefore are not

capable to conforming to a changing terrain. The foot portion of a high profile dynamic foot stays in the same position relative to the frame regardless of whether the amputee is walking on an incline, walking on uneven terrain or moving in a side-to-side direction.

The multiaxial dynamic feet of the prior art attempt to simulate motion of the ankle and are generally considered more stable than high profile dynamic feet. A disadvantage of the multiaxial dynamic foot is that generally it is a low profile prosthesis. By comparison to the high profile dynamic feet, low profile multiaxial dynamic feet can only store energy in their keel, which is a much smaller frame and, thus, a much smaller spring. Accordingly, there is correspondingly less energy storage. Therefore, with the prior art devices, there presently is a tradeoff between increased stability and improved energy storage capability.

Typically, the multiaxial feet of the prior art possess an axis of rotation through the ankle joint that lies transverse to the normal anterior-posterior alignment of the foot. Subsequently, such multiaxial prosthetic feet, although typically providing a range of rotation in an anterior-posterior direction, have limited freedom to move in a medial-lateral direction. Subsequently, the prior art multiaxial feet typically only allow a small amount of medial-lateral tilt and do not allow true rotation in the medial-lateral direction. Tilt is distinguishable from true rotation in that tilt may occur along any of a multitude of axes, whereas rotation occurs about one axis. Tilt may also be described as wobble. Typically, in the prior art devices, the amount of medial-lateral tilt is a consequence of some looseness in the ankle joint. This looseness is generally accomplished through the use of an elastomeric member in the ankle joint, which member can then compress to a limited degree, thus accommodating medial-lateral tilt. However, it can be difficult to control the tilting motion. Generally, the prior art devices do not possess an axis of rotation through an ankle joint where the axis of rotation lies in the anterior-posterior direction. Furthermore, elastomeric member tends to wear out.

Some of the prior art prosthetic feet provide a range of motion in an anterior-posterior direction. Providing this range of motion is accomplished, for example, by providing a flexible foot that includes an ankle member that flexes in the anterior-posterior direction. Another prior art device provides anterior-posterior motion by using a very high modulus material that permits limited deformation under a high load. This high modulus elastic material is typically positioned between the foot and the frame. As the load on the frame changes during the normal transfer of

weight that occurs during walking, the high modulus elastic material flexes to a limited extent. Still another prior device uses an o-ring positioned at the end of the frame where the frame connects to the foot. This o-ring is typically made of a high modulus material and will deform to a limited extent as weight is transferred during a normal stride.

5 Typical among the devices that rely on a high modulus elastic material for flexibility, the range of motion is necessarily limited. If the material forming at least part of the connection between the frame and the foot has too low a modulus, then control over the foot during normal walking will be compromised. Some of the prior art suggests that a limited degree of medial-lateral movement will occur as a result of the compression of the high modulus elastomeric material positioned between the frame and the foot. Such movement has been described in the art as a slight rocking or a slight tilting motion. The prior art further teaches that although some medial-lateral rocking motion can be accomplished, generally, medial-lateral movement is resisted.

10 Still another prior art device provides an elastomeric bushing about a heel ankle connector pin. As with the other prior art devices already described, this bushing material is a high modulus elastomer. Accordingly, some compression of the elastomer may take place during the normal weight transfer accompanying walking and result in a small amount of medial-lateral tilt or wobble. As provided above, prostheses that rely on a high modulus elastic material for flexibility tend to have a problem with durability because they wear out with repeated loading and unloading.

15 Lack of a true hinge allowing rotation in the medial-lateral direction is a disadvantage. True control of movement in a medial-lateral direction about a unitary axis is difficult to achieve in the prior art devices. Any medial-lateral movement in these devices is limited to a tilting movement. This tilting movement can occur along any of an infinite number of axes. Because it is not possible to control every possible axis along which the prior art foot may move, medial-lateral directional control can be difficult to achieve and, therefore, medial-lateral movement is typically constrained. Not surprisingly, the prior art devices limit a full range of medial-lateral movement. For example, in many prior art multiaxial feet, movement of the foot occurs through compression of an elastomeric pad positioned in the ankle region of the foot. Thus in order to provide movement of the foot in a medial-lateral direction the entire elastomeric pad must be of a

modulus that affects movement in all directions. In such a multiaxial foot, there is no independent control over movement in a singular direction or line of action.

It would therefore be an advantage to have a prosthetic foot that offered the stability advantages of a multiaxial dynamic foot with the energy storage capabilities of a high profile dynamic foot. It would be an even further advantage to have a prosthetic foot that allows true medial-lateral rotation. It would be at an even further advantage to have an adjustable prosthetic foot that would allow the manufacturer or wearer to select a range of medial-lateral rotation best suited to a wearer's needs.

It would be an even further advantage to have a high profile multiaxial prosthetic foot that could allow free rotation about an axis that lies in the anterior-posterior direction.

Summary of the Invention

In accordance with the principals of the present invention, there is provided a high profile multiaxial prosthetic foot providing rotation of a footplate in a medial-lateral direction.

According to one embodiment, the high profile multiaxial prosthetic foot includes a tubular frame connected to a footplate using a spring connector. In embodiments of the present invention, the spring connector may include a high modulus elastic material, a torsional spring or combinations of these. Thus, the present invention provides a high profile multiaxial prosthetic foot that includes a high profile component and a multiaxial component.

The present invention also provides a high profile multiaxial dynamic prosthetic foot having an adjustable range of medial-lateral rotation. The medial-lateral rotation of the prosthetic foot of the present invention may be adjusted to accommodate the individual needs of the wearer.

The present invention provides a prosthetic foot including: a frame having a first axis and a second axis; a connector connected to the frame, the connector being adapted to rotate about the first axis; and a footplate attached to the connector.

Thus, it will be seen that according to principals of the present invention there is provided a prosthetic foot that provides both the energy storage capabilities of a high profile prosthesis with the stability of a multiaxial prosthesis. The high profile multiaxial prosthetic foot of the present invention provides medial-lateral rotation as compared to the slight medial-lateral tilting

or rocking of the prior art devices. In a preferred embodiment, the medial-lateral rotation is controlled about a unitary axis. Furthermore, the high profile multiaxial prosthetic foot of the present invention provides a true hinge in the ankle joint region.

Embodiments of the present invention further provide a high profile multiaxial prosthetic foot having an ankle joint wherein the axis of rotation lies along the longitudinal axis of the foot. The prosthetic foot of the present invention further provides the capability of free rotation about the ankle joint about its axis of rotation.

Description of the Drawings

FIGURE 1 is a side view of an embodiment of the high profile multiaxial prosthetic foot made in accordance with the principles of the present invention.

FIGURE 2 is a schematic showing an end view of the high profile multiaxial prosthetic foot of FIGURE 1.

FIGURE 3 is a side view of the frame of FIGURE 1.

FIGURE 4 is an end view of one embodiment of a frame/connector/footplate assembly made in accordance with the principles of the present invention.

FIGURE 5 is an end view of an alternative embodiment of a frame/connector/footplate assembly made in accordance with the principles of the present invention.

FIGURE 6 is another embodiment of a frame/connector/footplate assembly made in accordance with the principles of the present invention.

FIGURE 7 is an end cross-sectional view of another embodiment of a high profile multiaxial prosthetic foot made in accordance with the principles of the present invention.

FIGURE 8 is an end cross-sectional view of the high profile multiaxial prosthetic foot made in accordance with the principles of the present invention illustrating means for rotation control.

FIGURE 9 is an embodiment of a high profile multiaxial prosthetic foot made in accordance with the principles of the present invention showing alternate connector means and means for rotation control.

FIGURE 10 is a side view of still another embodiment of a high profile multiaxial prosthetic foot made in accordance with the principles of the present invention.

FIGURE 11 is a side view of still another embodiment of a high profile multiaxial prosthetic foot made in accordance with the principles of the present invention.

FIGURE 12 is an end view of a high profile multiaxial prosthetic foot made in accordance with the principles of the present invention showing rotation of the prosthetic foot about an axis aligned with the longitudinal axis of the foot.

FIGURE 13 is an end view of a high profile multiaxial prosthetic foot made in accordance with the principles of the present invention showing rotation of the prosthetic foot about an axis aligned with the longitudinal axis of the foot.

FIGURE 14a is a side view of a high profile multiaxial prosthetic foot made in accordance with the principles of the present invention showing an adjustable displacement of a frame with respect to the foot.

FIGURE 14b is a side view of a high profile multiaxial prosthetic foot made in accordance with the principles of the present invention showing an adjustable displacement of a frame with respect to the foot.

FIGURE 15 is an end view of a high profile multiaxial prosthetic foot made in accordance with the principles of the present invention showing the displacement of a frame with respect to the vertical alignment of a residual limb.

5 Detailed Description of the Invention

10 In FIGURE 1, a high profile multiaxial prosthetic foot ("prosthetic foot") made in accordance with the principles of the present invention is labeled 10. The prosthetic foot 10 includes a frame 12, a connector 15 and a footplate 19. An upper portion of the frame 12 may be connected to socket (not shown) that is connected to a leg of the human wearer of the prosthetic foot 10 and a lower portion of the frame 12 is adapted to connect to the footplate 19. In a preferred embodiment, the frame 12 has a generally circular cross-section. Of course, other suitable cross-sections may be used. The connector 15 is adapted to allow rotation of the frame 12 about an axis that is aligned with the longitudinal axis of the footplate 19. As shown in FIGURE 2, an ankle joint 23 defines the connection between the frame 12 and the connector 15. The footplate 19 is attached to the connector 15, and, preferably, the footplate 19 is rigidly attached to the connector 15. Thus, it can be seen that the footplate 19 is free to rotate about an axis defined by the ankle joint 23, the axis of rotation lying along the longitudinal axis of the footplate 19 and the lower portion of the frame 12. The prosthetic foot 10 may also be adapted for anterior-posterior movement, by, for example, providing means for the elastic deformation of the connector 15, the frame 12, and/or the footplate 19. Thus, the prosthetic foot 10 may provide multiaxial movement.

The frame may be constructed of a high strength polymer or a composite material such as a carbon fiber laminate, for example. In a preferred embodiment, the frame is an L-shaped member. Being a generally L-shaped member, the frame defines a first axis and a second axis. 25 The footplate may also be constructed of a high strength polymer or a composite material such as a carbon fiber laminate.

In FIGURE 3, the frame 12 is depicted removed from the connector 15. The frame 12 may be described as having a generally long axis L1 along the upper portion of the frame 12 and a generally short axis S1 along the lower portion of the frame 12, however, long axis L1 and 30 short axis S1 may be of any length as required by a wearer of the prosthetic foot 10. The short

axis S1 is connected to the connector 15 through the ankle joint 23. In one embodiment, when the prosthetic foot 10 is assembled, the short axis S1 is aligned with the longitudinal axis of the footplate 19.

FIGURES 4, 5 and 6 show alternative embodiments of the present invention and more particularly, show alternative means for connecting a frame to a footplate. In FIGURE 4, a frame 42 is connected to a connector 45 through an ankle joint 43. The connector 45 may be any general shape so long as it does not preclude the utility of the prosthetic foot 10. The connector 45 is generally configured so that it may provide an ankle joint 43 having an axis of rotation that lies along an anterior-posterior direction. The connector 45 is attached to the footplate 49. In this embodiment, the connector 45 is adapted to frictionally receive the frame 42. Thus, medial-lateral rotation of the frame 42 about its short axis is limited by the coefficient of friction existing between the connector 45 and the frame 42 at the ankle joint 43. The connector 45 may be made of any suitable material that preserves the functionality of the prosthetic foot 10. For example, a high strength polymer, a carbon fiber laminate or a high modulus elastomeric material may be used for the connector 45. A high modulus elastomeric material, for example, may allow movement of the footplate 49 in an anterior-posterior direction via compression of the connector 45.

In FIGURE 5, an alternative embodiment of the connector of the present invention is illustrated. Frame 52 is connected to a spring 55 through an ankle joint 53. Spring 55 is then attached to a footplate 59. In the embodiment depicted in FIGURE 5, connector 55 is in the form of a torsional spring. However, other spring designs, such as a leaf spring, may be used. The spring 55 is generally configured so that it may provide an ankle joint 43 having an axis of rotation that lies along an anterior-posterior direction. The spring 55 may be constructed of a carbon fiber laminate or metal, for example. Thus, the amount of rotation of the footplate 59 about the ankle joint 53 may be limited by the spring constant for the spring 55. In this embodiment, it is preferred that the frame 52 be fixedly attached to the spring 55 at the ankle joint 53. However, it may be possible to allow rotation of the short axis of the frame 52 within the ankle joint 53 with respect to the spring 55, by providing that the spring 55 is adapted to frictionally receive the frame 52. Thus, the amount of rotation of the footplate 59 about the

ankle joint 53 is limited both by the coefficient of friction existing between the short axis of the frame 52 and the spring 55 at the ankle joint 53 and also the spring constant of the spring 55.

In FIGURE 6, yet another embodiment of a frame/connector/footplate assembly made in accordance with the principles of the present invention illustrated. In FIGURE 6, a frame 62 is connected to a spring 65 at an ankle joint 63. In the embodiment depicted in FIGURE 6, spring 65 is in the form of a torsional spring. However, other spring designs, such as a leaf spring, may be used. The spring 65 is generally configured so that it may provide an ankle joint 63 having an axis of rotation that lies along the short axis of the frame 62. The spring 65 may be constructed of a carbon fiber laminate or metal, for example. Thus, the amount of rotation of the footplate 69 about the ankle joint 63 may be limited by the spring constant for the spring 65. In this embodiment, a connector 64 is also used. The spring 65 and the connector 64 are both attached to the footplate 69. Rotation of the frame 62 within the ankle joint 63 may be constrained by providing that the spring 65 is adapted to frictionally receive the frame 62. Rotation of the frame 62 within the connector 64 may be constrained by providing that the connector 64 is adapted to frictionally receive the frame 62. The rotation of the footplate 69 may be limited by the coefficient of friction between the frame 62 and the spring 65, the coefficient of friction between the frame 62 and the connector 64, or the spring constant of the spring 65, or combinations thereof.

In FIGURE 7, a cross-sectional end view of a high profile multiaxial prosthetic foot 70 is shown. In this embodiment, the frame 72 is connected to a spring 74 by a setscrew 73. The setscrew 73 may fixedly attach the spring 74 to the frame 72 and limit or even prevent the rotation of the frame 72 within the spring 74. A connector 75 is adapted to rotationally receive the frame 72. The connector 75 is attached to the footplate 79. The spring 74 may abut the footplate 79.

In FIGURE 8, a cross-sectional end view of another embodiment of a prosthetic foot of the present invention is shown. In this embodiment, a control element 81 is adapted to receive a frame 82. Rotation stop 87, 88 extend from control element 81. Also shown are a connector 85 and a footplate 89. The rotation of the footplate 89 about its axis is limited by the rotation stop 87, 88. The footplate 89 may rotate either clockwise or counter-clockwise until reaching the rotation stop 87, 88. It will be recognized that there are other adaptations of the rotation

adjustment means provided by the rotation stop 87, 88 and the control element 81. The structure of the rotation stop 87, 88 and the control element 81, and the related function of rotation control, are further described below with respect to FIGURE 9.

In FIGURE 9, a side-view of a prosthetic foot incorporating a connector 75, a spring 74 and a control element 81. The frame 72 is connected to a spring 74 by a setscrew 73. The connector 75 is adapted to rotationally receive the frame 72. The connector 75 is also attached to the footplate 79 in a known manner. The spring 74 may abut the footplate 79. The control element 81 is adapted to receive the frame 72. In the preferred embodiment, the control element 81 is rigidly attached to the frame 72. The control element includes a rotation stop 87. The rotation of the footplate 89 about its axis is limited by the rotation stop 87. A second rotation stop may be included as described above. The footplate 89 may rotate either clockwise or counter-clockwise until reaching a rotation stop.

In FIGURE 10, yet another embodiment of a prosthetic foot of the present invention is illustrated. In this embodiment, a frame 112 is connected to a connector 115, which in turn is attached to a footplate 119. In this embodiment, the footplate 119 is formed to allow the use of a frame 112 wherein the angle between the short axis and the long axis of the frame 112 is greater than 90°.

In FIGURE 11, yet another embodiment of a prosthetic foot of the present invention is illustrated. In this embodiment, a frame 112 is rotatably connected to a connector 115, which in turn is fixedly attached to a footplate 119. The frame 112 is connected to a spring 114. The spring 114 may abut the footplate 119. In this embodiment, the footplate 119 is formed to allow the use of a frame 112 wherein the angle between the short axis and the long axis of the frame 112 is greater than 90°.

FIGURE 12 illustrates the ability of a prosthetic foot made in accordance with the principles of the present invention to provide medial-lateral rotation. In FIGURE 12, an end view of the prosthetic foot 10 is shown. As described in the previous embodiments, a frame 12 is connected to a connector 15 at an ankle joint 13 with the connector 15 being attached to a footplate 19. In FIGURE 12, the prosthetic foot is positioned on an inclined plane 11. This is analogous to a wearer of a prosthetic foot standing sideways on a hill. Thus, the longitudinal axis of the footplate 19 is transverse to the direction of incline of the incline plane 11. It can be

seen that the high profile multiaxial prosthetic foot of the present invention allows rotation in a medial-lateral direction, thus, stabilizing the footplate 19 in such a position.

FIGURE 13 likewise illustrates an embodiment of a prosthetic foot of the present invention positioned on an inclined plane 11. In FIGURE 13, there is further defined an angle θ . The angle θ is the angle formed between the plane of the incline and the long axis of the frame 12. Because of the orientation of the ankle joint 13, θ may effectively vary between 0 and 180°.

The prosthetic foot of the present invention may be adapted to provide adjustment of a frame with respect to a connector and a footplate. In FIGURE 14a and FIGURE 14b, for example, a frame 112 is shown connected to a connector 115. The connector 115 is attached to a footplate 119. One end of the footplate 119 defines an imaginary vertical line v . A distance x_1 is defined by the separation distance between v and the long axis of the frame 112. By positioning the long axis of the frame 112 closer to the connector 115 a second distance x_2 may be defined between v and the long axis of the frame 112. The distance x_1 is less than the distance x_2 . Thus, the position of the long axis of the frame 112 may be adjusted with respect to the connector 115 and the footplate 119. Along its longitudinal axis, the footplate 119 defines a first end and a second end. Thus the position of the long axis of the frame 112 may be adjustably located with respect to the first end or the second end of the footplate 119. The adjustable positioning of the frame 112 with respect to the footplate 119 may accomplished, for example, by adjustably connecting the frame 112 to the connector 115. Thus, the short axis of the frame 112 may be moved to a desired position along the longitudinal axis of the footplate 119 and then fixed in position by the connector 115 with respect to further movement along the longitudinal axis of the footplate. Referring to FIGURE 7, in one embodiment for example, the frame 72 may be adjustably positioned with respect to the footplate 79 as described above and this position fixed by tightening setscrew 73.

In FIGURE 15, for example, a frame 112 is shown connected to a connector 115. The connector 115 is attached to a footplate 119. Further illustrated is a residual limb 120. As known in the art, the residual limb is attached to a socket that is attached to the frame 112. The residual limb 120 defines a generally vertical axis v_1 . An angle θ_1 is defined by the long axis of the frame 112 and v_1 . Thus it can be seen that θ_1 may be varied to allow the residual limb 120 to be offset with respect to the footplate 119. The footplate 119 can be seen to also define a top

plane and a bottom plane. As illustrated in FIGURE 15, the connector 115 is attached to the footplate 119 at the top plane of the footplate 119. Thus, the long axis of the frame 112 may be adjustably positioned with respect to the top plane so that the long axis defines an angle with respect to the top plane that is different than 90°. Referring to FIGURE 7, in one embodiment for example, the frame 72 may be adjustably positioned with respect to the footplate 79 as described above and this position fixed by tightening setscrew 73.

As is known in the art, the footplate of the prosthetic foot of the present invention may be covered with an anthropomorphic flexible polymer in the shape of a foot.

The high profile multiaxial prosthetic foot made in accordance with the principles of the present invention allows free rotation of a prosthetic footplate about an axis that lies along the longitudinal axis of the footplate. Thus, such a prosthetic foot provides free rotation from 0 to 180° in a medial-lateral direction. A high profile multiaxial prosthetic foot made in accordance with the principles of the present invention further provides means to control the amount of rotation of the footplate. Thus, the present invention provides a high profile multiaxial prosthetic foot that allows true medial-lateral rotation as opposed to mere medial- lateral tilt.

There has been provided in accordance with the present invention, a high profile multiaxial prosthetic foot providing stability for the user in conditions requiring medial-lateral rotation. While the invention has been described with specific embodiments, many alternatives, modifications and variations will be apparent to those skilled in the art in light of the forgoing description. Accordingly, it is intended to include all such alternatives, modifications and variations set forth within the spirit and scope of the appended claims.

What is claimed is:

1. A prosthetic foot comprising:
a frame having a first axis and a second axis;
a connector connected to the frame, the connector being adapted to rotate about the first
5 axis; and
a footplate attached to the connector, the footplate defining a first end and a top plane.
2. The prosthetic foot of Claim 1 wherein the frame is a tubular L-shaped member.
- 10 3. The prosthetic foot of Claim 1 wherein the frame is manufactured from a material, the material selected from the group consisting of a high strength polymer and composite material.
- 15 4. The prosthetic foot of Claim 1 wherein the connector is manufactured from a material, the material selected from the group consisting of a high modulus elastomeric material, a high strength polymer and a composite material.
5. The prosthetic foot of Claim 1 wherein the connector is a torsional spring.
- 20 6. The prosthetic foot of Claim 5 wherein the torsional spring is a metal torsional spring.
7. The prosthetic foot of Claim 5 wherein the torsional spring is a carbon fiber laminate composite.
8. The prosthetic foot of Claim 1 wherein the second axis of the frame is adjustably
25 positioned with respect to the first end of the footplate.
9. The prosthetic foot of Claim 1 wherein the second axis of the frame is adjustably
positioned with respect to the top plane of the footplate.

10. A prosthetic foot comprising:
a frame;
a connector rotatably connected to the frame;
5 a footplate attached to the connector, the footplate defining a longitudinal axis such that the longitudinal axis is a rotation axis of the footplate about the frame; and
means for controlling the rotation of the footplate about the frame, the rotation controlling means being adapted to be attached to the frame.

11. The prosthetic foot of Claim 10 wherein the frame is a tubular L-shaped member.

12. The prosthetic foot of Claim 11 wherein the frame is manufactured from a material, the material selected from the group consisting of a high strength polymer and composite material.

13. The prosthetic foot of Claim 10 wherein the connector manufactured from a material, the material selected from the group consisting of a high modulus elastomeric material, a high strength polymer and a composite material.

14. The prosthetic foot of Claim 10 wherein the connector is a torsional spring.

15. The prosthetic foot of Claim 14 wherein the torsional spring is a metal torsional spring.

16. The prosthetic foot of Claim 14 wherein the torsional spring is a carbon fiber laminate composite.

17. The prosthetic foot of Claim 14 wherein the rotation controlling means includes a control element and at least one rotation stop.

18. A prosthetic foot comprising:

a frame;

a connector connected to the frame such that the connector may rotate about the frame about an axis transverse to a medial-lateral direction of movement of the prosthetic foot; and

a foot plate attached to the connector.

19. The prosthetic foot of Claim 18 wherein the connector is manufactured from a material, the material selected from the group consisting of a high modulus elastomeric material, a high strength polymer and a composite material.

20. The prosthetic foot of Claim 18 wherein the connector is a torsional spring.

21. The prosthetic foot of Claim 18 further including means for controlling the rotation of the connector.

22. The prosthetic foot of Claim 21 wherein the rotation control means includes a control element and at least one rotation stop.

Abstract of the Invention

The present invention provides a prosthetic foot that provides both energy storage capabilities and stability. The prosthetic foot of the present invention provides medial-lateral rotation as compared to the slight tilting or rocking in the medial-lateral plane of the prior art devices. Furthermore, the prosthetic foot of the present invention provides a true hinge in the ankle joint region that may be adapted so that the degree of rotation is controlled.

5

Fig. 1

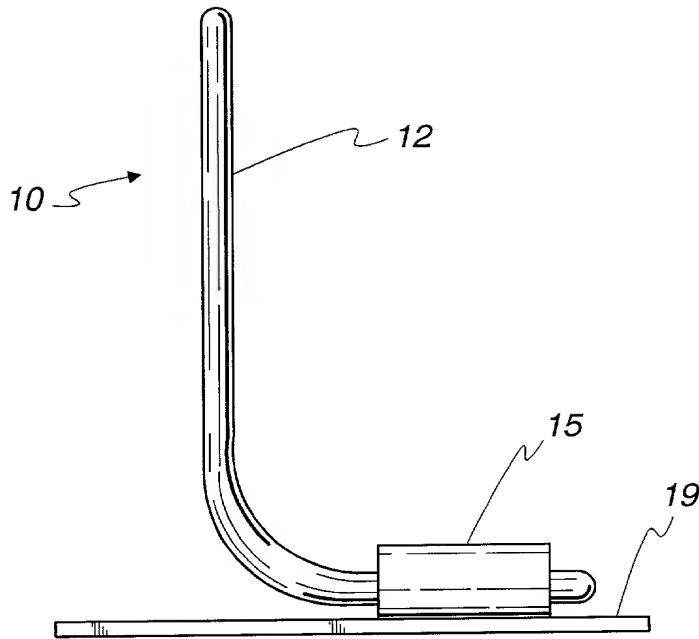


Fig. 2

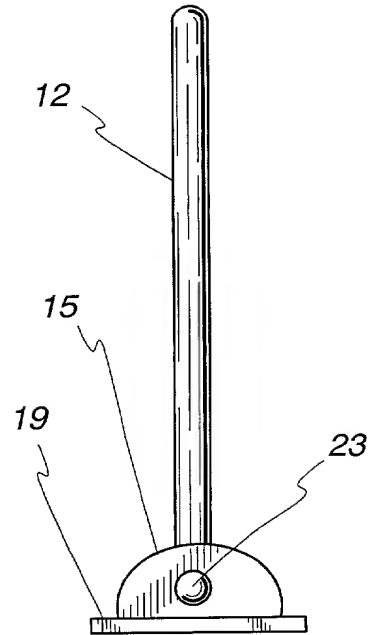


Fig. 3

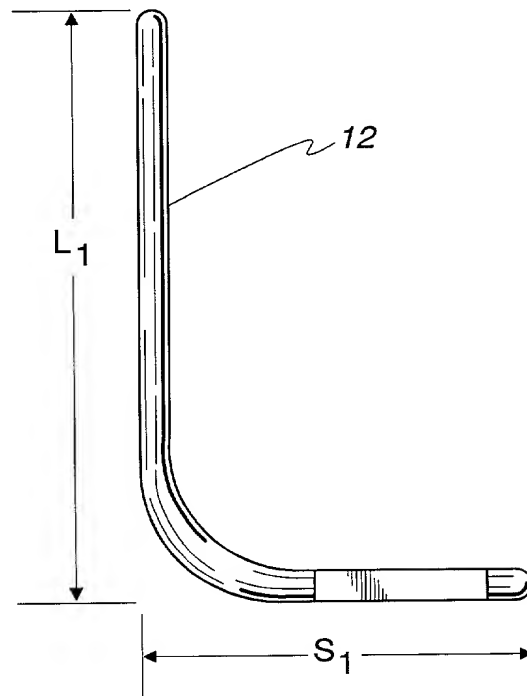


Fig. 4

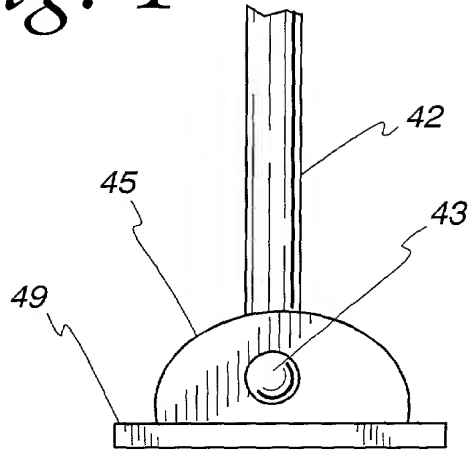


Fig. 5

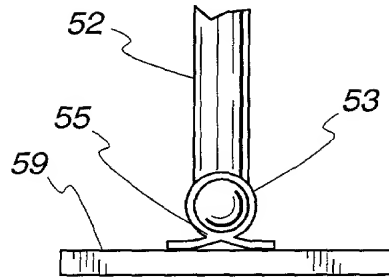


Fig. 6

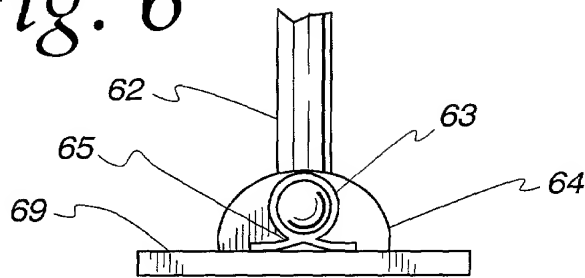


Fig. 7

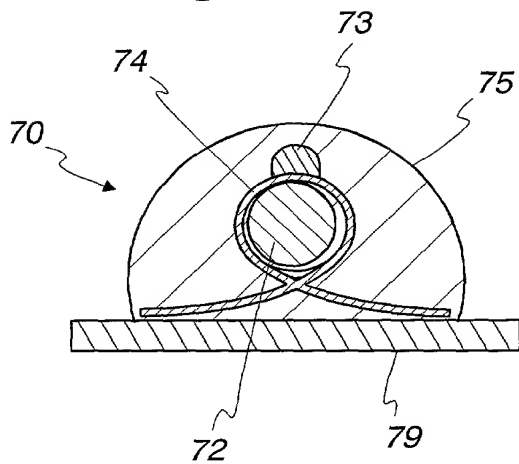


Fig. 8

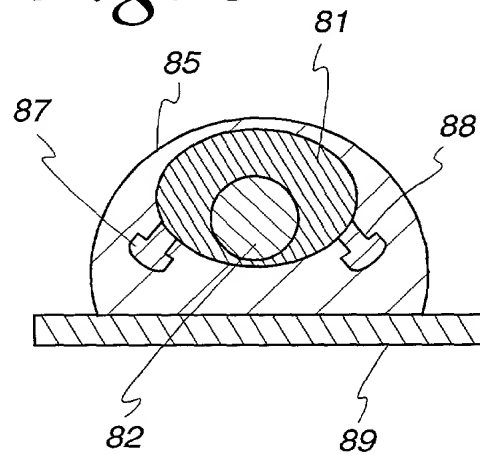


Fig. 9

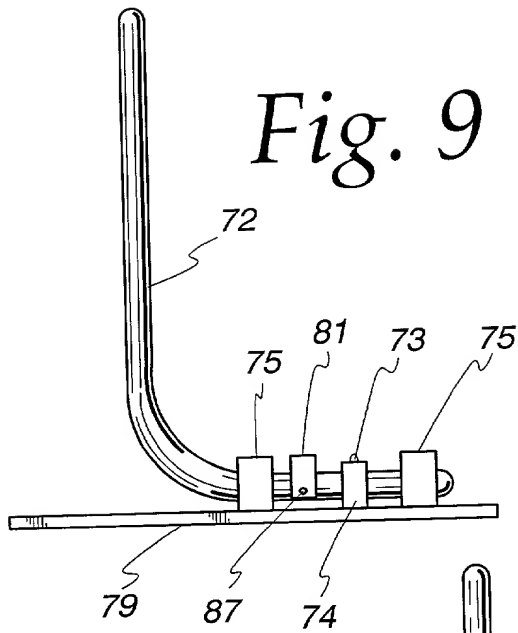


Fig. 10

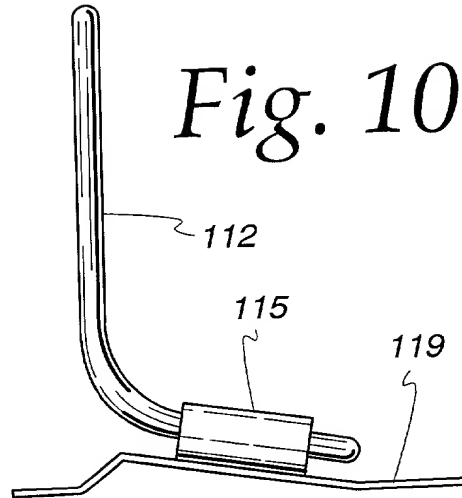


Fig. 11

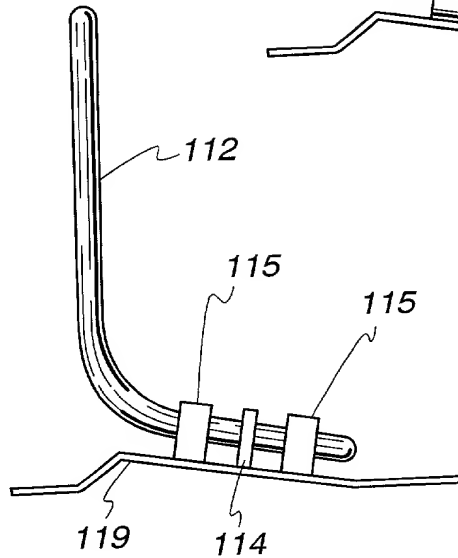


Fig. 12

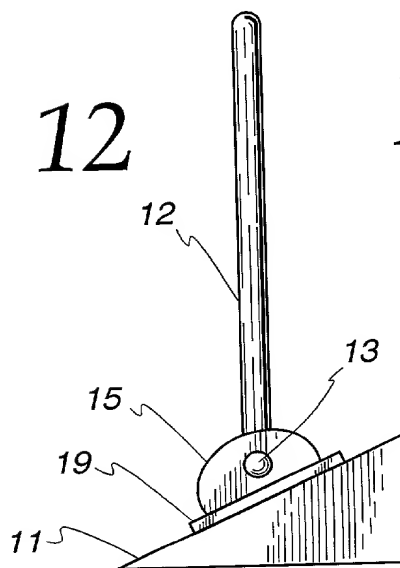
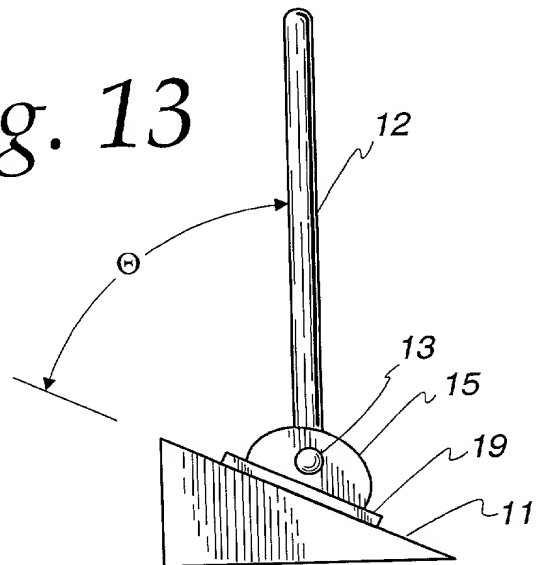


Fig. 13



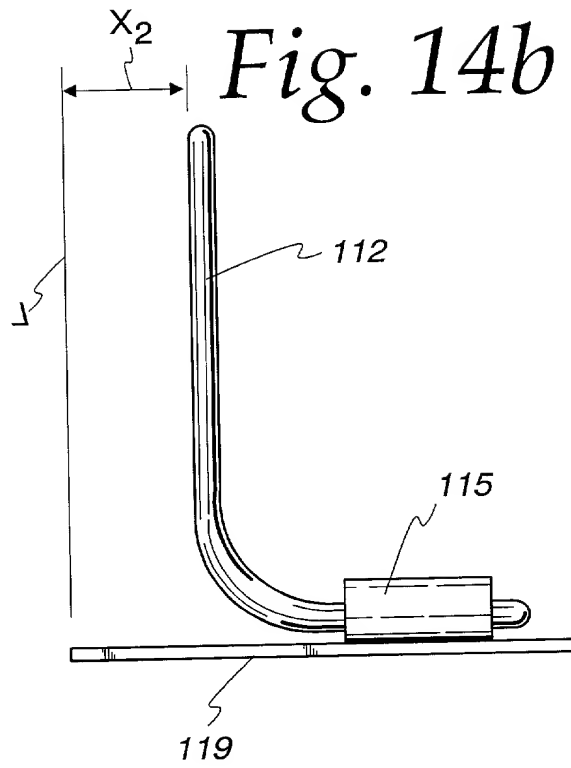
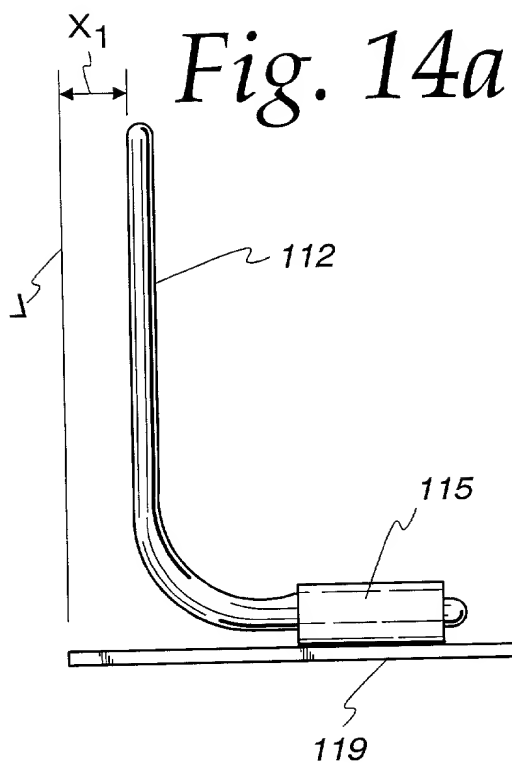
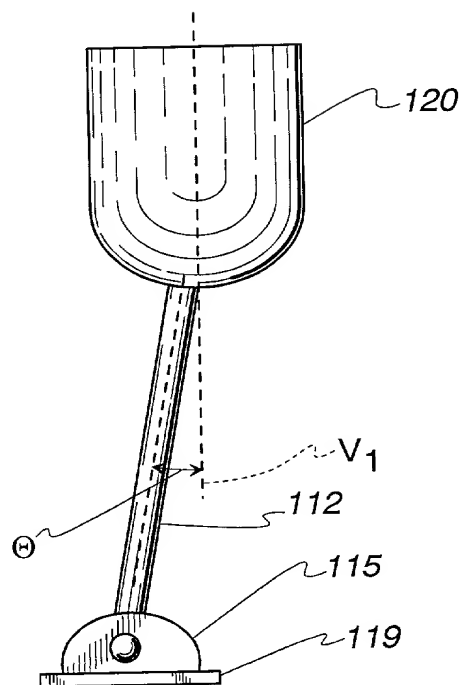


Fig. 15



Docket No.
P1308USA

Declaration and Power of Attorney For Patent Application

English Language Declaration

As a below named inventor, I hereby declare that:

My residence, post office address and citizenship are as stated below next to my name,

I believe I am the original, first and sole inventor (if only one name is listed below) or an original, first and joint inventor (if plural names are listed below) of the subject matter which is claimed and for which a patent is sought on the invention entitled

HIGH PROFILE MULTIAXIAL PROSTHETIC FOOT

the specification of which

(check one)

☒ is attached hereto.

☐ was filed on _____ as United States Application No. or PCT International Application Number _____ and was amended on _____

(if applicable)

I hereby state that I have reviewed and understand the contents of the above identified specification, including the claims, as amended by any amendment referred to above.

I acknowledge the duty to disclose to the United States Patent and Trademark Office all information known to me to be material to patentability as defined in Title 37, Code of Federal Regulations, Section 1.56.

I hereby claim foreign priority benefits under Title 35, United States Code, Section 119(a)-(d) or Section 365(b) of any foreign application(s) for patent or inventor's certificate, or Section 365(a) of any PCT International application which designated at least one country other than the United States, listed below and have also identified below, by checking the box, any foreign application for patent or inventor's certificate or PCT International application having a filing date before that of the application on which priority is claimed.

Prior Foreign Application(s)

Priority Not Claimed

(Number)

(Country)

(Day/Month/Year Filed)

☐

(Number)

(Country)

(Day/Month/Year Filed)

☐

(Number)

(Country)

(Day/Month/Year Filed)

☐

I hereby claim the benefit under 35 U.S.C. Section 119(e) of any United States provisional application(s) listed below:

(Application Serial No.)

(Filing Date)

(Application Serial No.)

(Filing Date)

(Application Serial No.)

(Filing Date)

I hereby claim the benefit under 35 U. S. C. Section 120 of any United States application(s), or Section 365(c) of any PCT International application designating the United States, listed below and, insofar as the subject matter of each of the claims of this application is not disclosed in the prior United States or PCT International application in the manner provided by the first paragraph of 35 U.S.C. Section 112, I acknowledge the duty to disclose to the United States Patent and Trademark Office all information known to me to be material to patentability as defined in Title 37, C. F. R., Section 1.56 which became available between the filing date of the prior application and the national or PCT International filing date of this application:

(Application Serial No.)

(Filing Date)

(Status)
(patented, pending, abandoned)

(Application Serial No.)

(Filing Date)

(Status)
(patented, pending, abandoned)

(Application Serial No.)

(Filing Date)

(Status)
(patented, pending, abandoned)

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code and that such willful false statements may jeopardize the validity of the application or any patent issued thereon.

POWER OF ATTORNEY: As a named inventor, I hereby appoint the following attorney(s) and/or agent(s) to prosecute this application and transact all business in the Patent and Trademark Office connected therewith. *(list name and registration number)*

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